### Automatic Generation of Training Data for Brain Tissue Classification from MRI

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#### Brain tissue classification:

 $\Rightarrow$  the procedure of labeling each image voxel as a tissue class.



4 classes: CSF, Grey-matter, White-matter, "background"



Main problem: subject different than anatomical model.





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#### **Outline:**

- Requirements
- Existing methods
- Our method
- Validation and results

## Target application:

- Quantitative measurements, such as:
  - normalized tissue/structure volume
  - atrophy measures
  - voxel-based morphometry
  - cortical surface
  - cortical thickness
  - •
- Studies on a large number of subjects (150 1000); data acquired at many different sites.

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- ACCURATE
  - application: quantitative measurements
- FULLY AUTOMATIC
  - reproducibility; many datasets to process
- ROBUST against variability in:
  - subject brain's morphology
  - MRI data: image contrast, artifacts, ...

### Existing methods:

- Kamber et al. (IEEE TMI '95)
- Van Leemput (IEEE TMI '99), Ashburner ("SPM-99")

 $\hookrightarrow$  all use a probabilistic brain anatomy atlas  $\to$  problems with brain anatomies significantly different than atlas.

### Existing methods: EM

EM-style schemes by Van Leemput (IEEE TMI '99), Ashburner ("SPM-99").

Drawback: assume multi-variate Normal ("Gaussian") intensity distributions.

 $\rightarrow$  poor assumption for multi-spectral brain aMRI ? biology, acquisition artifacts . . .

#### Existing methods: Kamber

Kamber (IEEE TMI '95) used Tissue Probability Maps (TPM), defined in a stereotaxic space.

- 1. subject MRI spatially registered to stereotaxic space (linear registration)
- 2. select MRI intensity samples from spatial locations very likely to contain a given tissue type
- 3. use these samples to train a supervised classifier (such as: Bayes, neural network, kNN, ...).

### Stereotaxic space TPM:

Subject MRI:







0%

100%

### Stereotaxic space TPM:

young normal



elderly, Alzheimer's Disease

young normal population









### Training samples selection:

 $\hookrightarrow$  choose spatial locations with TPM value  $\geq \mathcal{T}$ 



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 $\hookrightarrow$  choose spatial locations with TPM value  $\geq \mathcal{T}$ 



- lower T desired for more spatial coverage  $\Rightarrow$  robust estimation of tissue intensity distributions.
- higher T desired for reducing wrong class guesses.

### Our novel method:



Pruning : removal of samples with incorrect class labels.

#### Our novel method:

- accommodates subject anatomies significantly different than model
- non-parametric: no assumptions about feature space (intensity) distributions
- allows for a lower TPM  $\mathcal{T}$  $\Rightarrow$  better estimation of intensity distributions
  - $\Rightarrow$  accuracy, robustness

"raw" samples in feature space:





```
edge (i, j) is removed
if
length(i,j) > T \times A(i)
or if
length(i, j) > T \times A(j),
where A(i) = average
length of all other
edges incident
                     on
node i
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[Step 2]

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[Step 2]

cluster = a connected component of graph.

CSF cluster = cluster with most CSF samples. ...

Stop when BG, CSF, GM, WM clusters are distinct.



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[Step 3]

 $\Rightarrow$  discard samples that are not found in correct cluster.



#### Validation: simulated MRI

- T1-T2-PD multi-spectral simulated MRI, 10 different "elderly brain" phantoms
- young-normal model (TPM), N=53
- quantitative evaluation: Kappa = chance-corrected similarity measure between two image labelings (classifications). classified image ⇔ "gold standard" (phantom)

#### Validation: simulated MRI



(elderly brain simulated MRI, young-normal model)

### Validation: real MRI

- 1. young & normal individual (T1+T2+PD, and also T1 only), against full-brain manual segmentation.
- 2. 31 Ischemia patients (T1+T2+PD).
- 3. 11 Alzheimer's Disease (A.D.) elderly patients (T1+T2+PD).

#### **Results: Ischemia**







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### Results: A.D. elderly







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#### Future work:

Current limitations:

- inherent to intensity-only, discrete classification.
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 $\Rightarrow$  also use voxel neighbourhood information (e.g. image gradient), ...

### Summary:

- fully automatic brain tissue classification procedure.
- robust against anatomical variability.
- non-parametric: no assumptions about tissue intensity distributions (⇒ robust against imaging artifacts).
- validated qualitatively and quantitatively on simulated and on real MRI data.

#### Acknowledgements:

- John Sled, Steve Robbins, Peter Neelin, Godfried Toussaint, Noor Kabani, Louis Collins, Jean-François Mangin, Jason Lerch, Jennifer Campbell, Ives Levesque, Najma Khalili.
- the anonymous MICCAI-2002 reviewers.
- Alma Mater Student Travel Fund, Faculty of Graduate Studies and Research, McGill University, Montreal.

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